

Multiscale 3-D texture segmentation: Isotropic Representations

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Constructions

Collaborators & Acknowledgements

This work has been performed in collaboration with Simon K. Alexander (UH), Robert Azencott (UH and ENS) and Manos Papadakis (UH).

We gratefully acknowledge the contributions and previous related work by B.G. Bodmann (UH), S. Baid (formerly UH), D.J. Kouri (UH), X. Li (UH) and Juan R. Romero (U.Puerto Rico).

Outline

Background

- Biomedical Imaging and segmentation
- Segmentation flowchart

Mathematical Framework

- Feature Vectors
- Steerability
- Why frames and beyond

Isotropic Multiresolution Analysis

- Definition
- An Example of IMRA
- Directional selectivity

Spherical Harmonics

- 3-D Spherical Harmonics

Biomedical Imaging and segmentation

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- ▶ This assists diagnostic imaging especially when latent tissues are picked up by this process.
- ▶ A robust algorithm must be immune to rigid motions of the image.
- ▶ We require a multi-scale structure because textures manifest themselves at various scales.

Segmentation flowchart

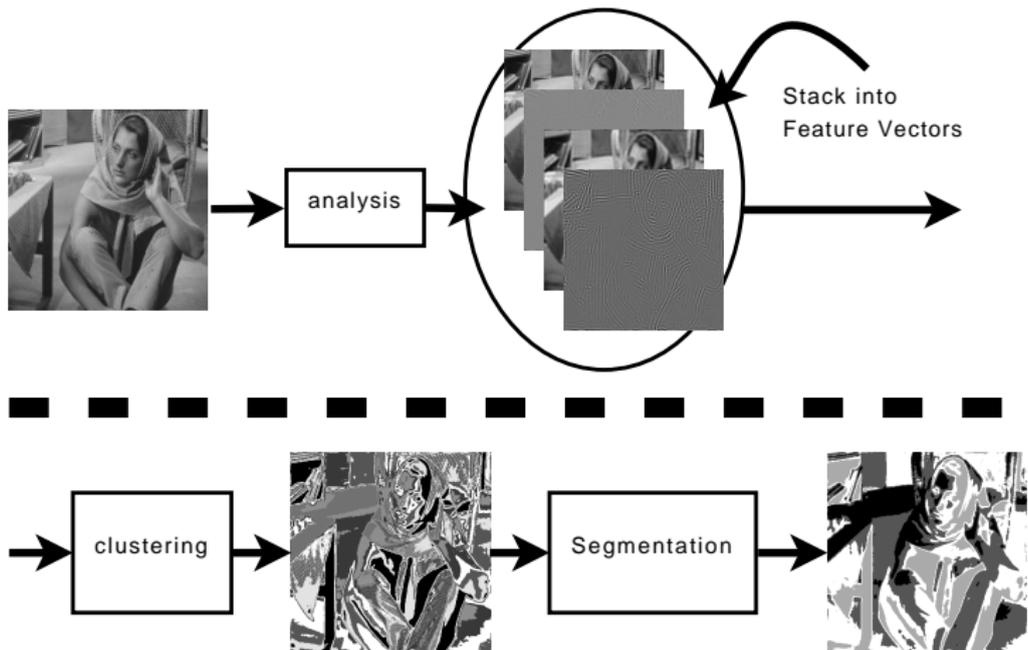


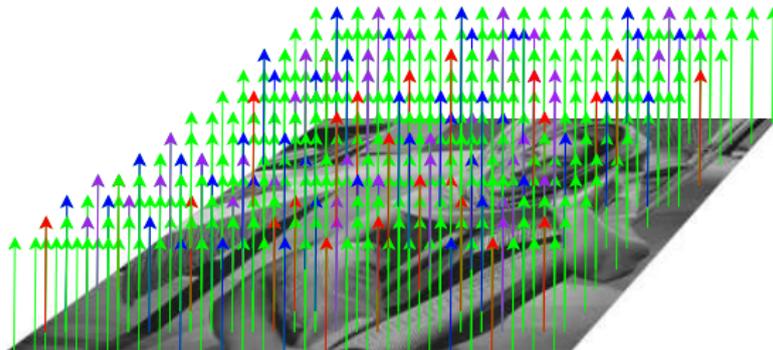
Image Lattice

For all $z \in \mathbb{R}^d$ associated data $f(z)$



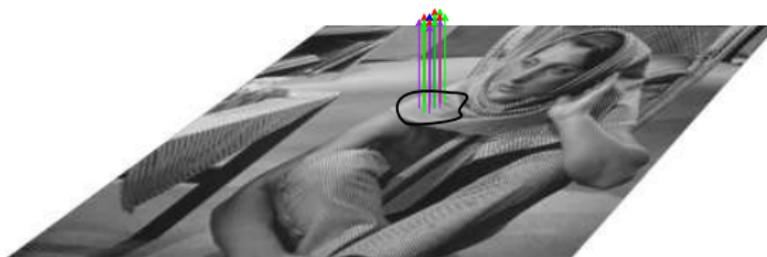
Feature Vectors on Image Lattice

Associated feature vectors $Af(z)$. Each vector co-ordinate is a wavelet coefficient.



Texture Patch

We care only about local Neighborhoods $\mathcal{N}(z)$ forming texture patches of related features



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- ▶ The vector space of all V -valued functions h defined on \mathbb{R}^3 such that $\|h(\cdot)\|$ is square integrable on \mathbb{R}^3 is denoted by H . Thus, $\|h\| = (\int_{\mathbb{R}^3} \|h(z)\|^2 dz)^{1/2}$.

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- ▶ Let $A : L^2(\mathbb{R}^3) \rightarrow H$ be a bounded linear transformation that associates to each f the V -valued function Af defined on \mathbb{R}^3 . This linear transformation is called a feature map.

Steerability

Definition

Consider a bounded linear feature mapping A generating for each image f and each voxel $z \in \mathbb{R}^3$ a feature vector $Af(z)$ in the Euclidean space V . We shall say that A is a *steerable feature mapping* if there is a mapping U from the group G of rigid motions into the general linear group $GL(V)$ of V such that for each rigid motion R of \mathbb{R}^3 , the invertible transformation $U(R)$ verifies,

$$A[\mathcal{R}f](z) = U(R) [Af(R(z))] \quad z \in \mathbb{R}^3.$$

Here \mathcal{R} is the following transformation induced by R on $L^2(\mathbb{R}^3)$:

$$\mathcal{R}f(z) = f(Rz).$$

Qualitative Requirements of feature vectors

We summarize the properties that the feature vectors should have:

- ▶ Efficient implementation (feature extraction must be feasible for volumes at least as large as $512 \times 512 \times 512$)

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- ▶ The features must provide localized information.
- ▶ A multi-scale structure to describe textures at different scales.

Hence, Multiresolution Analysis is an ideal choice.

Why not orthogonal wavelets?

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- ▶ Tensor product artifacts in higher dimensions.
- ▶ Inflexible design due to the orthogonality constraint.
- ▶ The segmentation algorithm needs approximately 5-15 dimensional feature vector space. This is hard to achieve with DWT using applicable length scales.

Problems with tensor product basis



Barb image

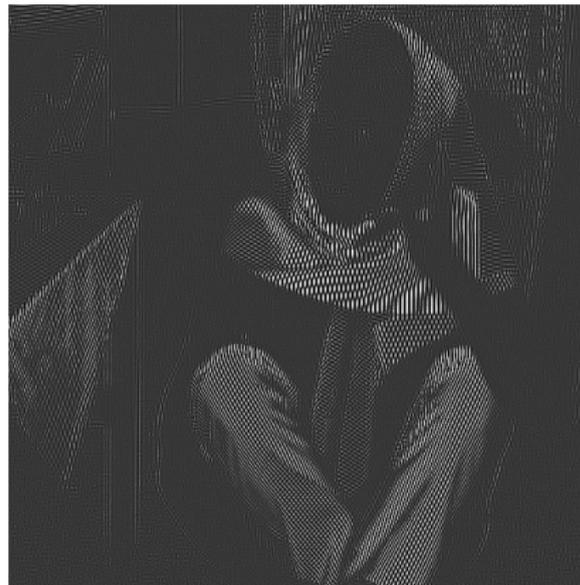


DB8 decomposition

Problems with tensor product basis

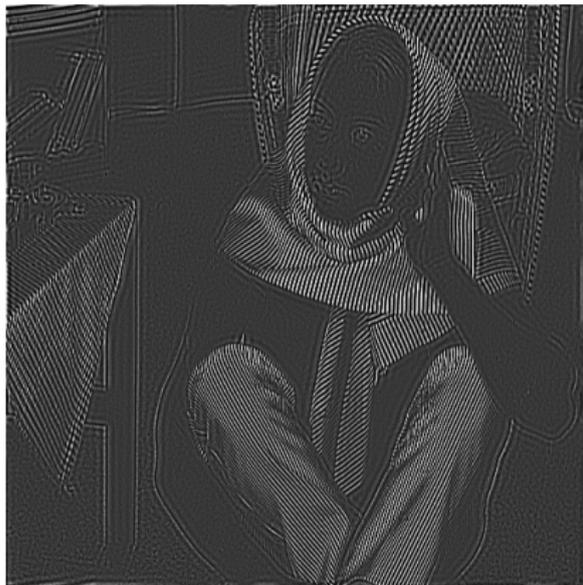


Barb image

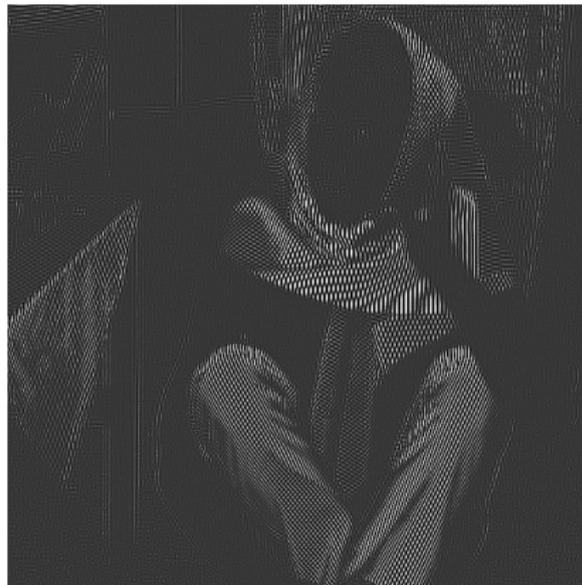


DB8 high pass

Problems with tensor product basis



IMRA high pass

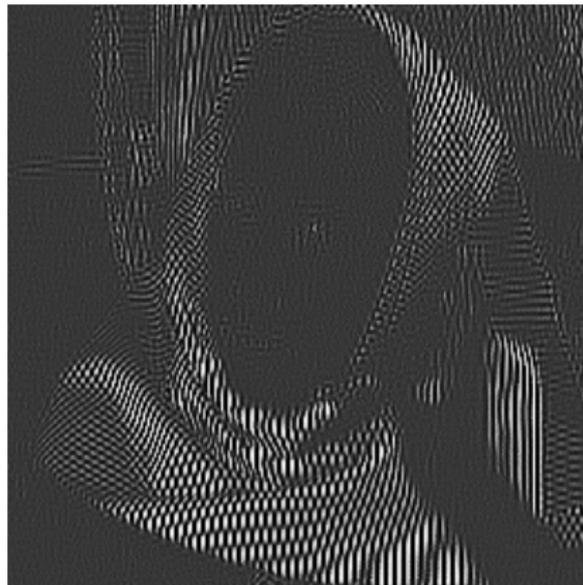


DB8 high pass

Problems with tensor product basis (Zoom)



IMRA high pass



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MRA properties

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- ▶ steerability

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Definition

An IMRA is a sequence $\{V_j\}_{j \in \mathbb{Z}}$ of closed subspaces of $L^2(\mathbb{R}^n)$ satisfying the following conditions:

- ▶ $\forall j \in \mathbb{Z}, V_j \subset V_{j+1}$,
- ▶ $(D)^j V_0 = V_j$,
- ▶ $\cup_{j \in \mathbb{Z}} V_j$ is dense in $L^2(\mathbb{R}^n)$,
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- ▶ V_0 is invariant under all rotations.

Then V_0 must be a Paley-Wiener space of a certain form, i.e. there exists a measurable set Ω invariant under all rotations such that

$$f \in V_0 \Leftrightarrow \hat{f}(\xi) = 0 \quad \xi \notin \Omega.$$

An example of IMRA

Let $\phi \in L^2(\mathbb{R}^d)$ a refinable function i.e. there exists $m_0 \in L^\infty(\mathbb{T}^d)$ such that

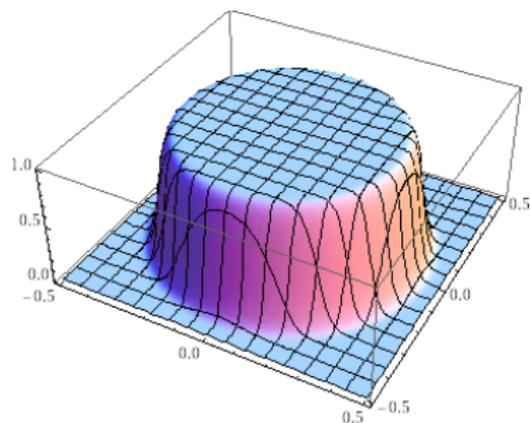
$$\hat{\phi}(2\cdot) = \hat{\phi}m_0.$$

We assume that $\hat{\phi}$ is smooth and satisfies the following:

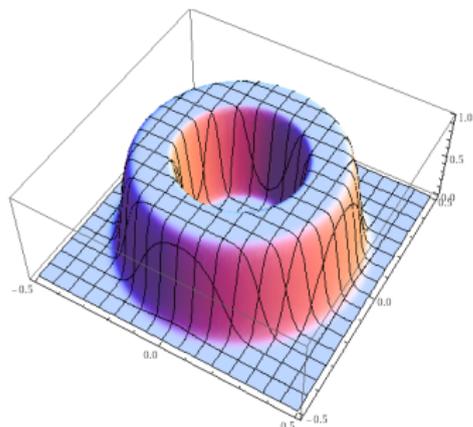
- ▶ $\hat{\phi}$ vanishes outside the ball centered at the origin with radius $r < 1/2$
- ▶ $\hat{\phi}(\xi) = 1$ for all ξ in the ball $B(0, \frac{1}{4})$

Define, ψ via $\hat{\psi}(2\cdot) = \hat{\phi} - \hat{\phi}(2\cdot)$.

2D IMRA scaling function and wavelet



(a) Fourier transform of the scaling function $\hat{\phi}$



(b) Fourier transform of the wavelet $\hat{\psi}(2.)$

Using the functions ϕ and ψ , we define the following feature map:

$$Af(z) = (\langle f, T_z\phi(\cdot/8) \rangle, \langle f, T_z\psi(\cdot/4) \rangle, \langle f, T_z\psi(\cdot/2) \rangle).$$

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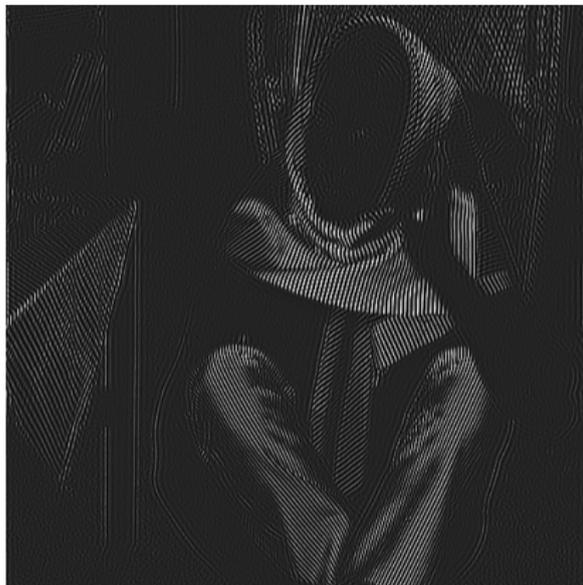
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- ▶ This map is both translation and rotation invariant
- ▶ Hence, it is steerable.

Directional Selectivity

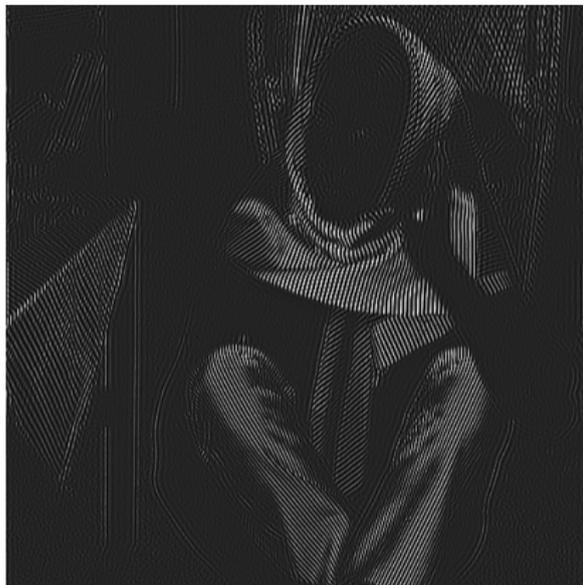


IMRA High Pass tensor $\sin(\theta)$

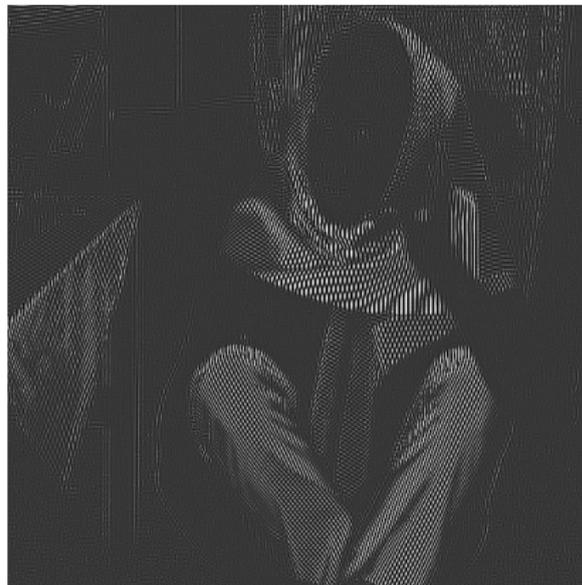


IMRA High Pass tensor $\cos(\theta)$

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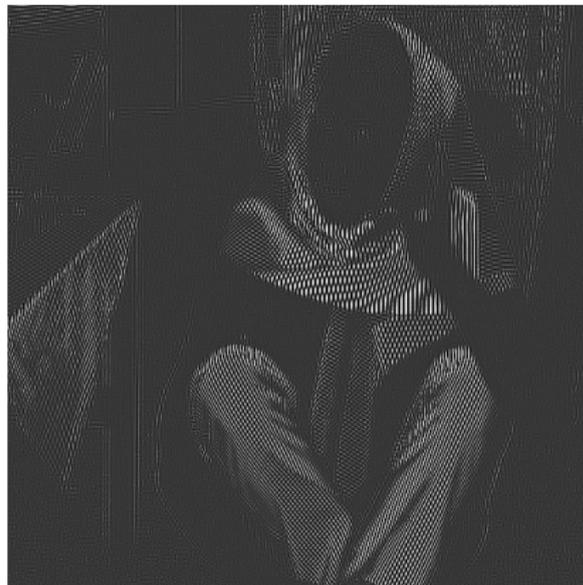


D8 High Pass

Better than tensor product basis

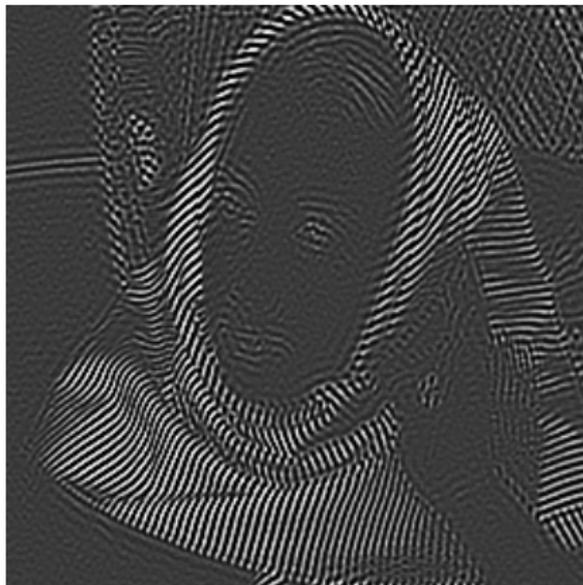


IMRA High Pass tensor $\cos(\theta)$

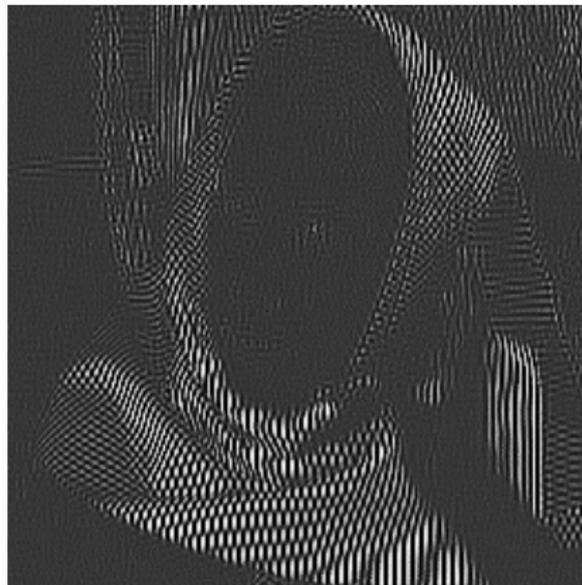


D8 High Pass

Better than tensor product basis (Zoom)

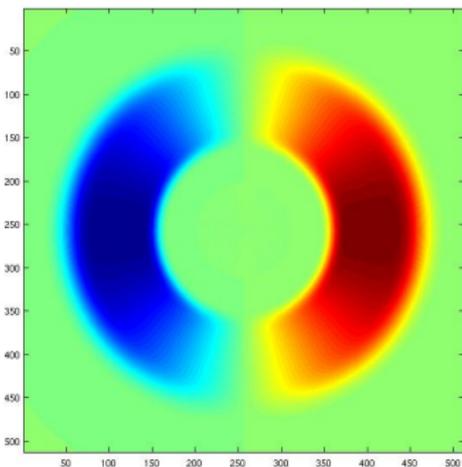


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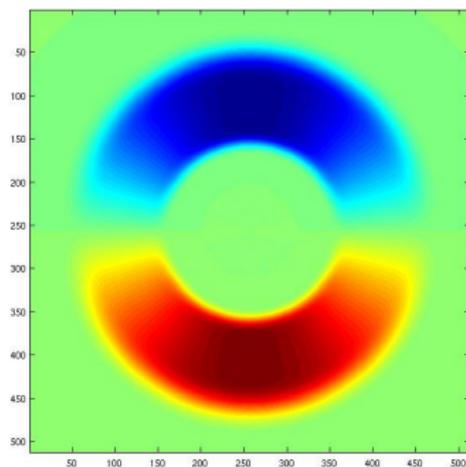


D8 High Pass

The filters



(c) High Pass tensor $\sin(\theta)$



(d) High Pass tensor $\cos(\theta)$

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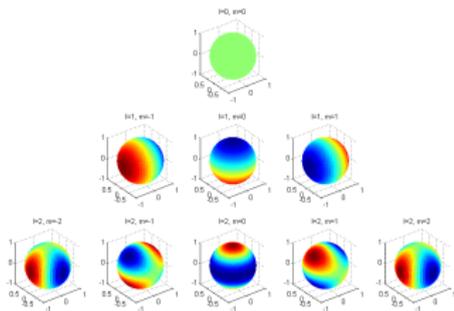
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- ▶ d_m is equal to 2 in the case of \mathbb{R}^2 or $2m + 1$ in the case of \mathbb{R}^3 .

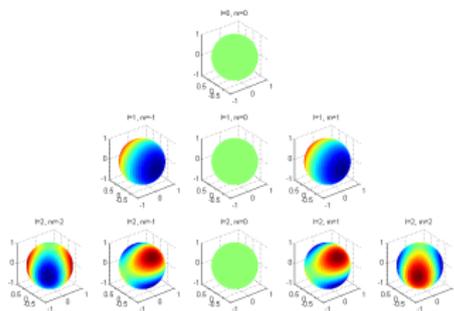
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- ▶ For $m = 0$ we only have $n = 0$ and $Y_{0,0} = 1$.

3D Spherical Harmonics of degree 0, 1 and 2

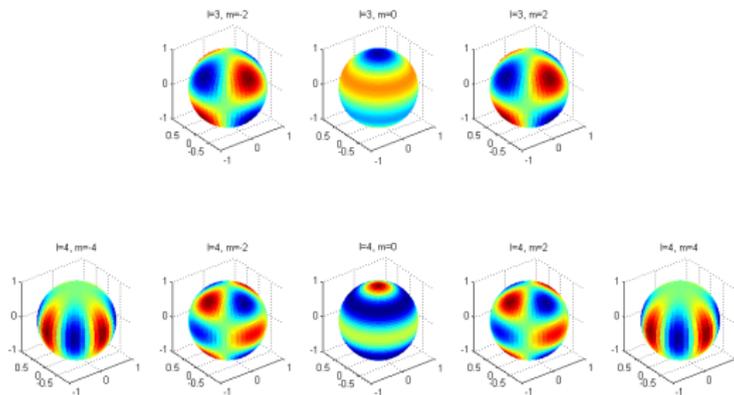


(e) Real part



(f) Imaginary part

More 3D Spherical Harmonics



(g) Real part of 3D Spherical Harmonics of degree 3 and 4

Thank you for your attention !!

References



S.D. Gertz, B.G. Bodmann, D. Vela, *et al.*

Three-dimensional isotropic wavelets for post-acquisitional extraction of latent images of atherosclerotic plaque components from micro-computed tomography of human coronary arteries.

Academic Radiology 14, 1509-1519.



S.K. Alexander, R. Azencott, M. Papadakis

Isotropic Multiresolution Analysis for 3D-Textures and Applications in Cardiovascular Imaging.

in Wavelets XII, SPIE Proceedings Vol. 6701, 2007.



J.R. Romero, S.K. Alexander, S. Baid, S. Jain, and M. Papadakis

The Geometry and the Analytic Properties of Isotropic Multiresolution Analysis.

submitted 2008.